

# Cellular and Molecular Biophysics

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***Corso di laurea in LM Biotecnologie Industriali- LM Fisica***

# FLUORESCENCE

I. Introduction to Fluorescence

II. Fluorochromes

III. Biological and biomedical applications



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# FLUORESCENCE



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I. Introduction to Fluorescence

II. Fluorochromes

III. Biological and biomedical applications

## BIOLOGICAL APPLICATIONS

- **TECHNIQUES IN FLUORESCENCE FOR LIVE CELL IMAGING**
  - Studies of molecular interactions in live cells  
(FRET)
  - Studies of molecular dynamics in live cells  
(FRAP-FLIP-FLAP)

## BIOMEDICAL APPLICATIONS

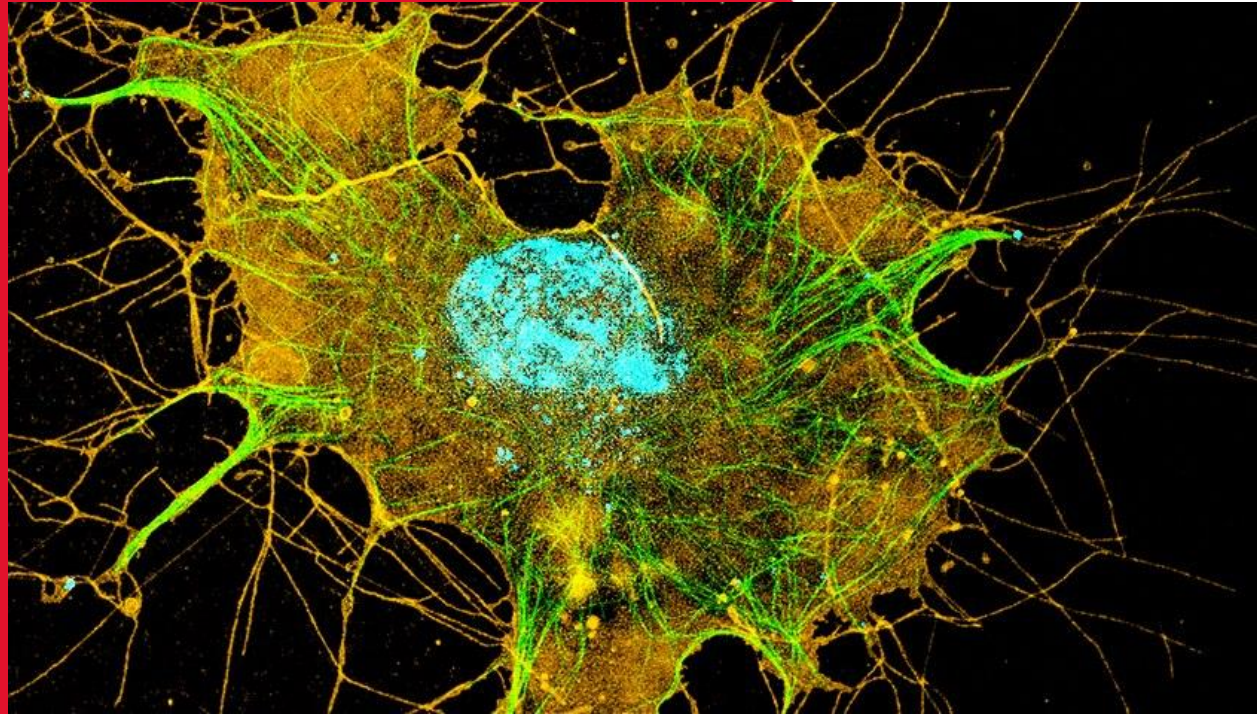
- **DIAGNOSTIC TOOLS FOR *IN VIVO* IMAGING**
- **PHOTODYNAMIC THERAPY**

# TECHNIQUES IN FLUORESCENCE FOR LIVE CELL IMAGING



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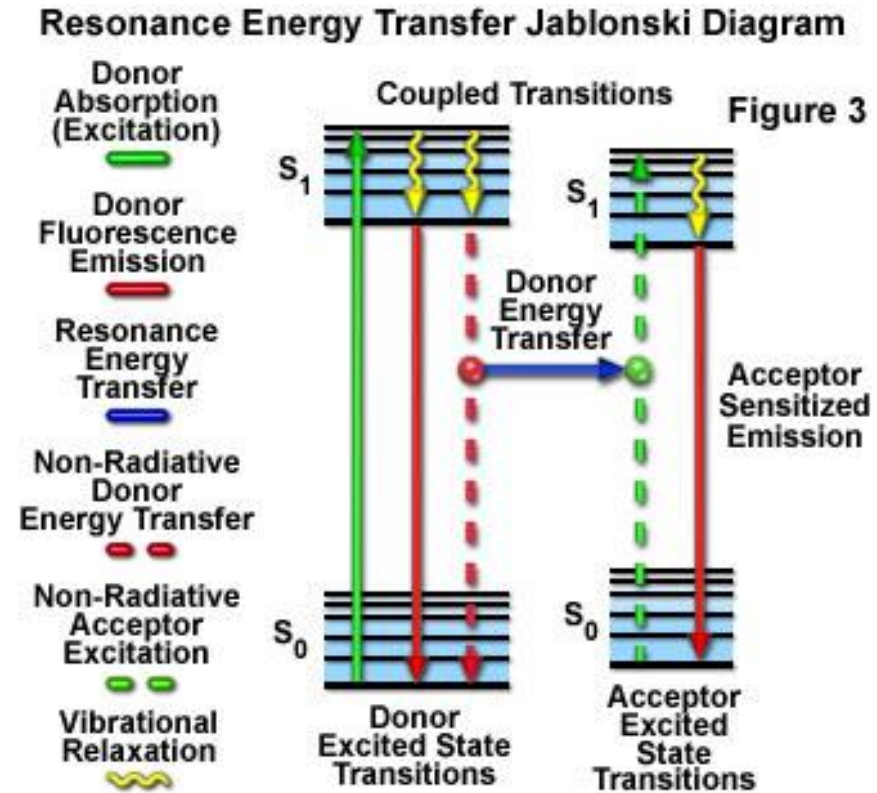


- Studies of molecular interactions in live cells

## FRET: Förster Resonance Energy Transfer

FRET is a quantum-mechanical phenomenon that occurs when two fluorochromes are in molecular proximity. It describes an energy transfer mechanism between two chromophores.

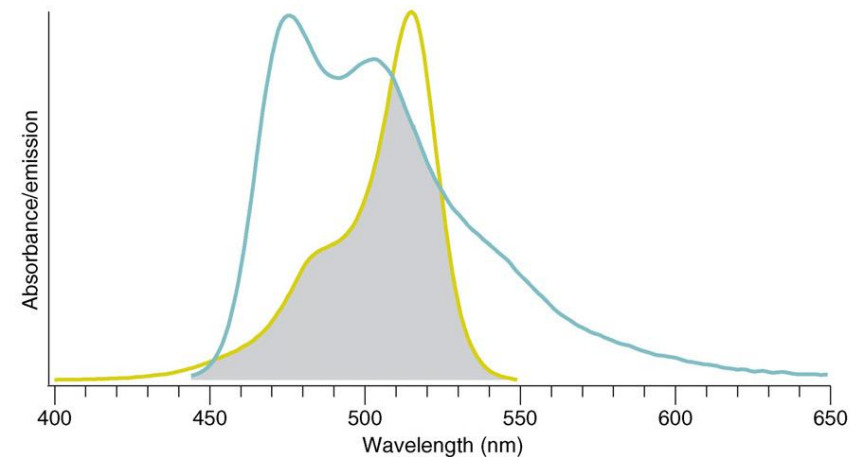
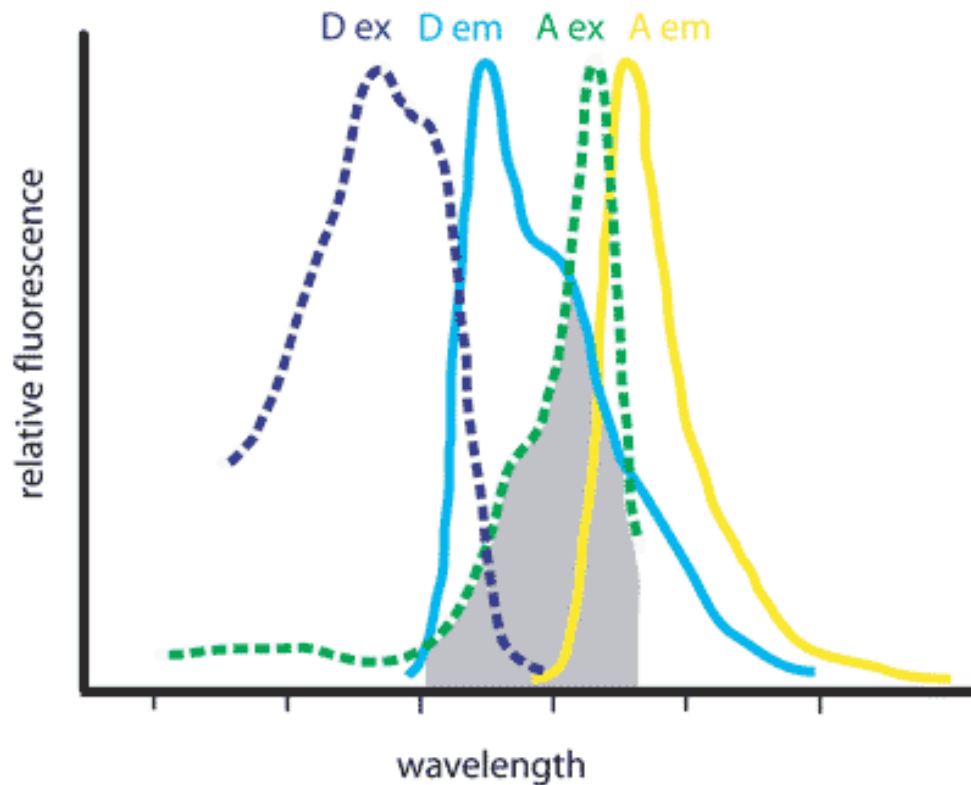
A **donor chromophore** in its **excited state** can **transfer energy** by a non radiative, long-range dipole-dipole coupling mechanism **to an acceptor chromophore in close proximity** (typically < 10 nm). This energy transfer mechanism is termed "Förster resonance energy transfer" (FRET), named after the German scientist: Theodor Förster.



<http://www.invitrogen.com/site/us/en/home/References/Molecular-Probes-The-Handbook/Technical-Notes-and-Product-Highlights/Fluorescence-Resonance-Energy-Transfer-FRET.html>

# FRET: Förster Resonance Energy Transfer

The emission spectrum of the donor fluorophore should overlap the excitation spectrum of the acceptor fluorophore.



# FRET: Förster Resonance Energy Transfer

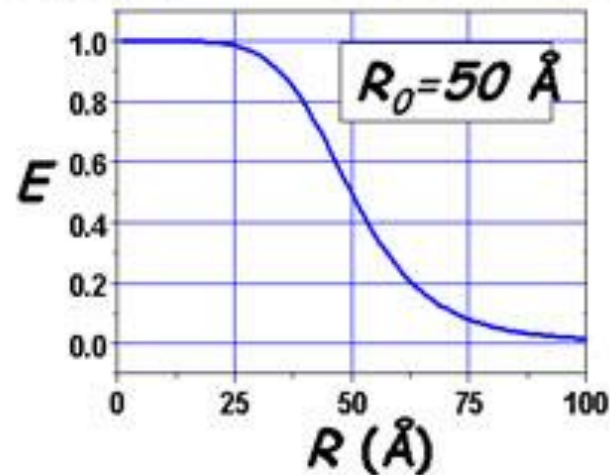
FRET is well-suited to the study of protein protein interactions, which occur on a similar spatial scale.



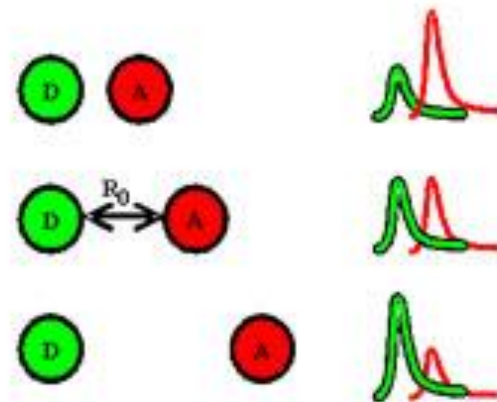
Energy Transfer Efficiency

$$E = \frac{1}{1 + (R/R_0)^6}$$

$R_0$  = 50% transfer efficiency distance  
3nm~7nm



“Spectroscopic Ruler”





# FRET: Förster Resonance Energy Transfer

$R_0$  can be calculated for any pair of fluorescent molecules.

The Förster distance **depends on the overlap integral of the donor emission spectrum with the acceptor absorption spectrum and their mutual molecular orientation** as expressed by the following equation:

$$R_0^6 = 8.8 \times 10^{-28} k^2 n^{-4} Q_0 J$$

$k^2$  = dipole orientation factor (often assumed as 2/3 when both the dyes are freely rotating and can be considered to be isotropically oriented during the excited state lifetime)

$n$  = refractive index of the medium

$Q_0$  = fluorescence quantum yield of the donor in the absence of the acceptor

$J$  = spectral overlap integral

$$J = \int f_D(\lambda) \epsilon_A(\lambda) \lambda^4 d\lambda$$

$f_D$  = normalized donor emission spectrum

$\epsilon_A$  = acceptor molar extinction coefficient

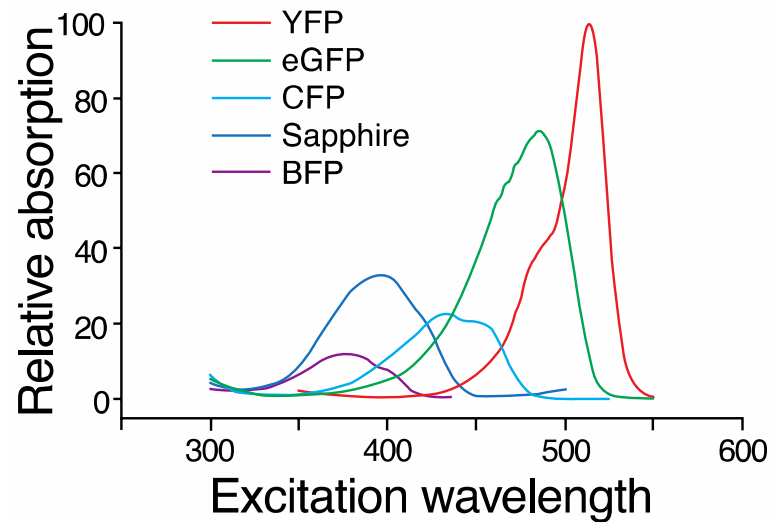
## Characteristics to take in account when choosing GFPs for FRET

- 1) **Excitation spectra** of the two dyes have to be **sufficiently separated** in order to stimulate the donor selectively
- 2) The **emission spectrum of the donor fluorophore** should **overlap the excitation spectrum of the acceptor fluorophore** in order to obtain efficient energy transfer
- 3) **Reasonable separation in emission spectra** between donor and acceptor GFPs is required to allow the fluorescence of each chromophore to be measured independently

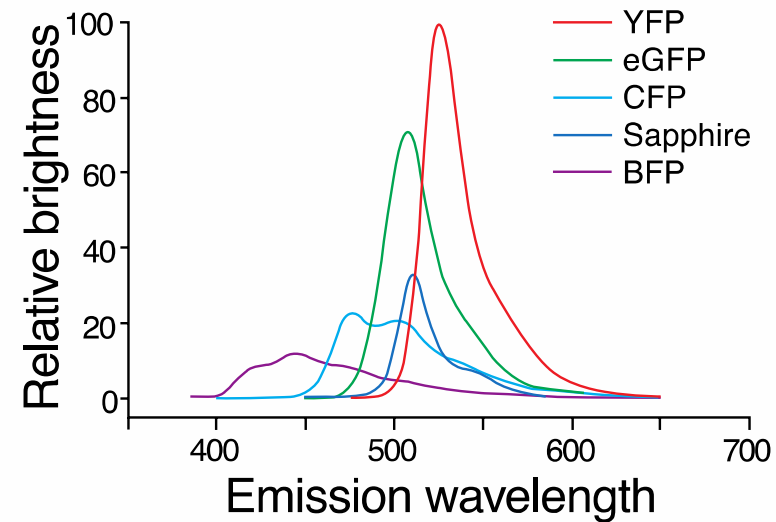
# Characteristics to take in account when choosing GFPs for FRET

## GFPs for FRET

(a) Excitation spectra



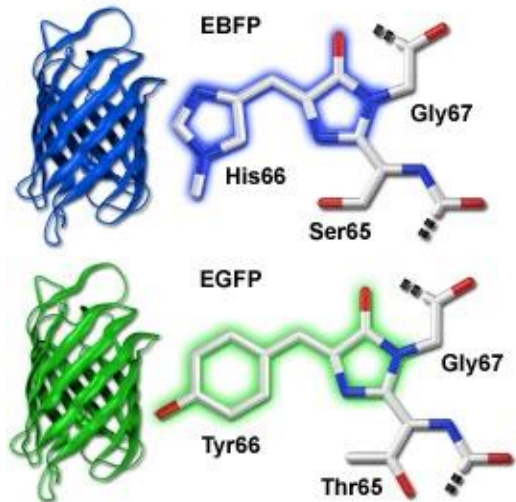
(b) Emission spectra



# Characteristics to take in account when choosing GFPs for FRET

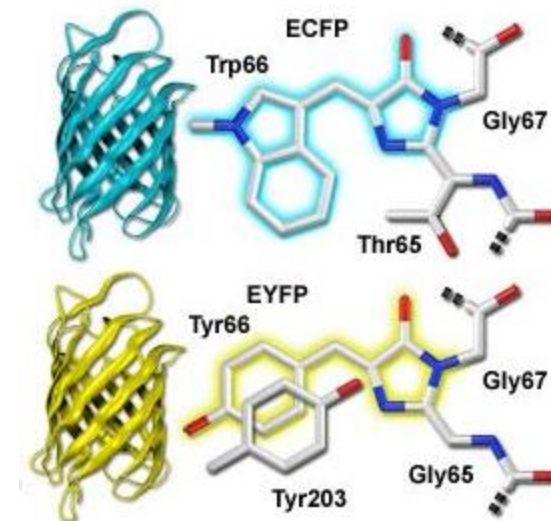
## GFPs for FRET

### EBFP-EGFP



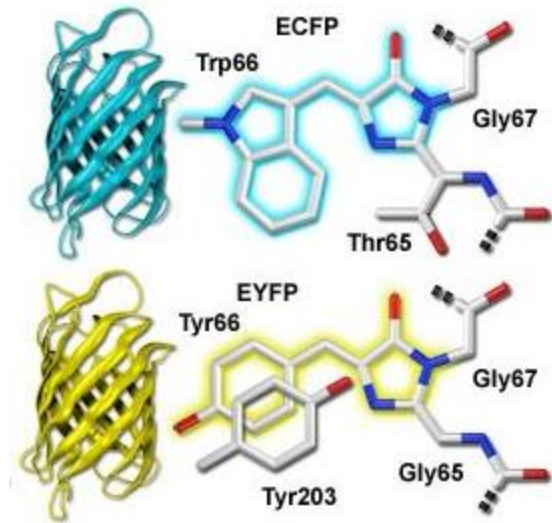
Poor photophysical properties of EBFP is a serious limitation to the use of this couple for FRET

### ECFP-EYFP



CFP-YFP is the best couple for FRET

# Characteristics to take in account when choosing GFPs for FRET



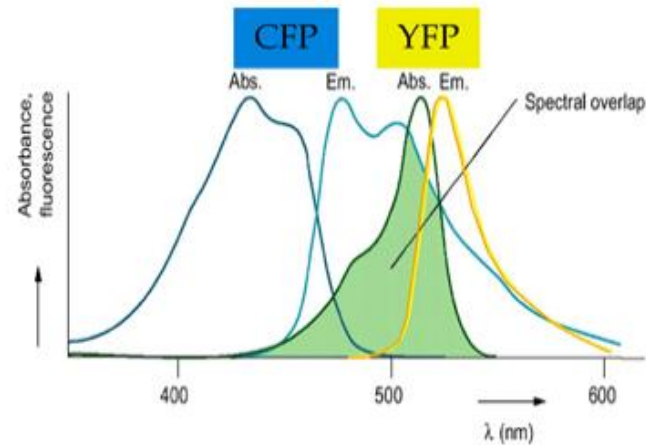
CFP - YFP

$\lambda_{ex}$  CFP = 405 nm

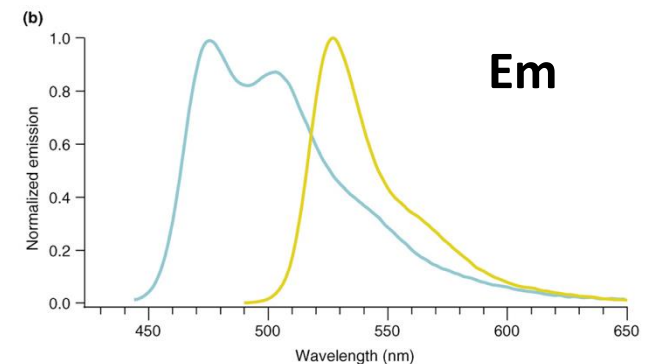
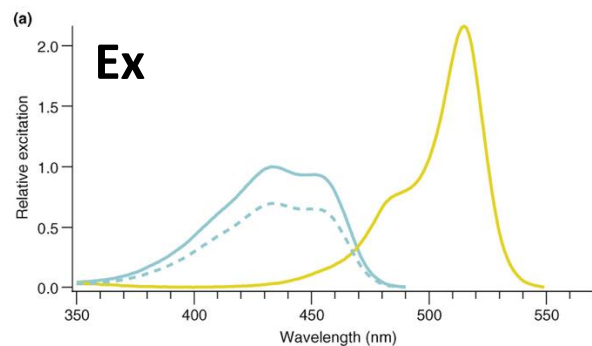
$\lambda_{em}$  CFP = 485 nm

$\lambda_{ex}$  YFP = 514 nm

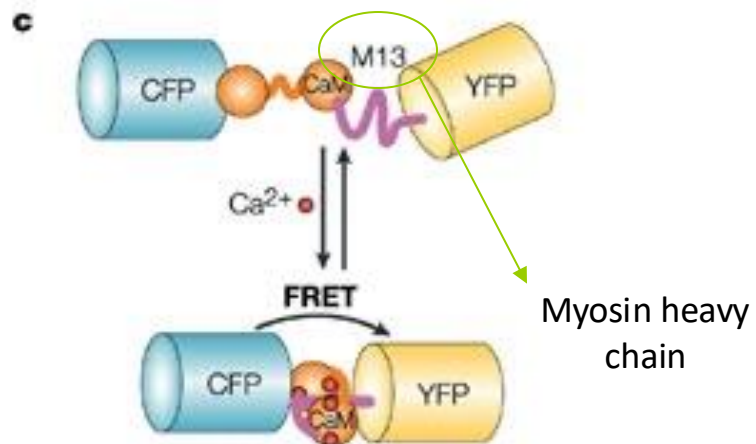
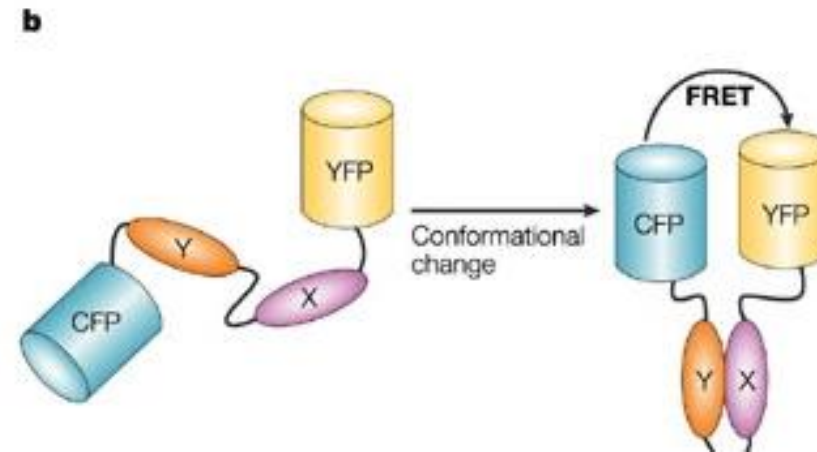
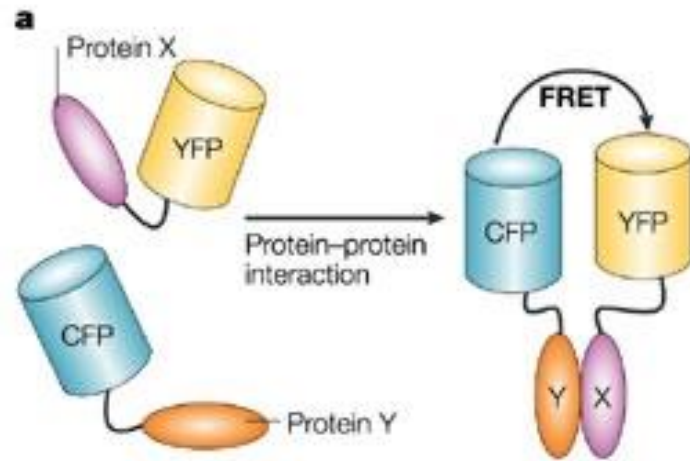
$\lambda_{em}$  YFP = 527 nm



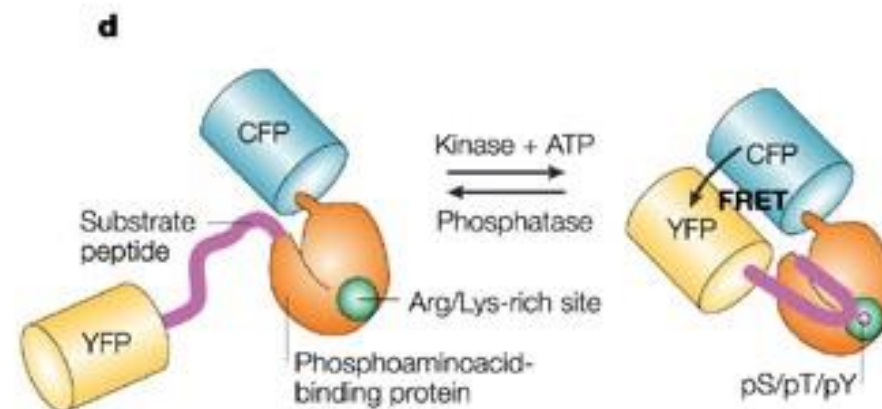
...although the significant cross-talk between both the excitation and emission spectra



# General design of FRET-based fluorescent probes



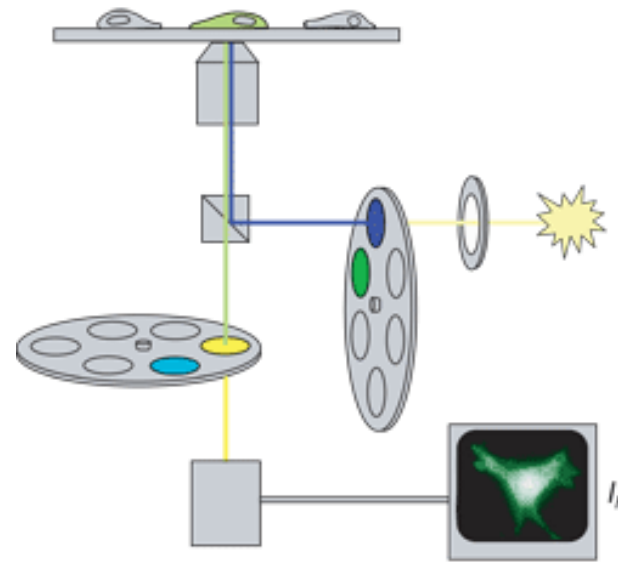
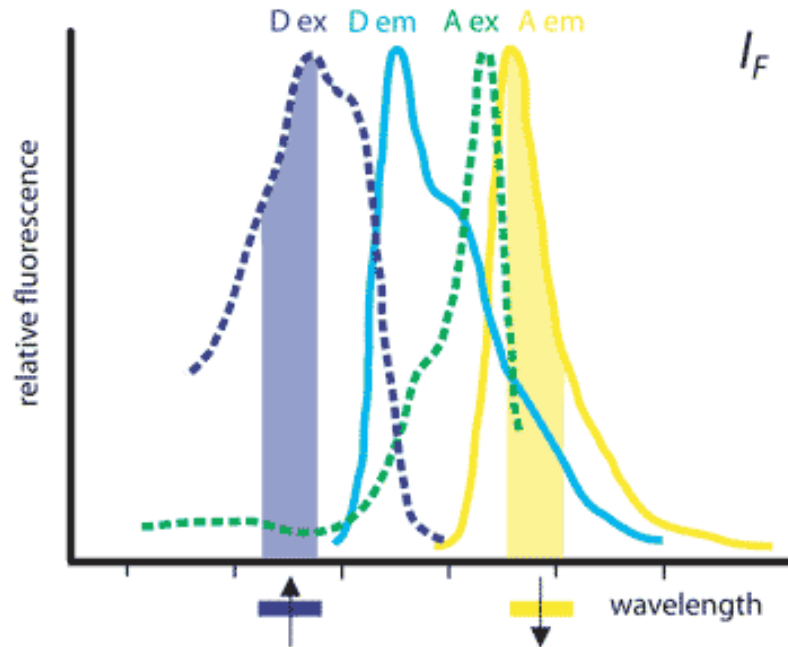
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# Methods for imaging FRET

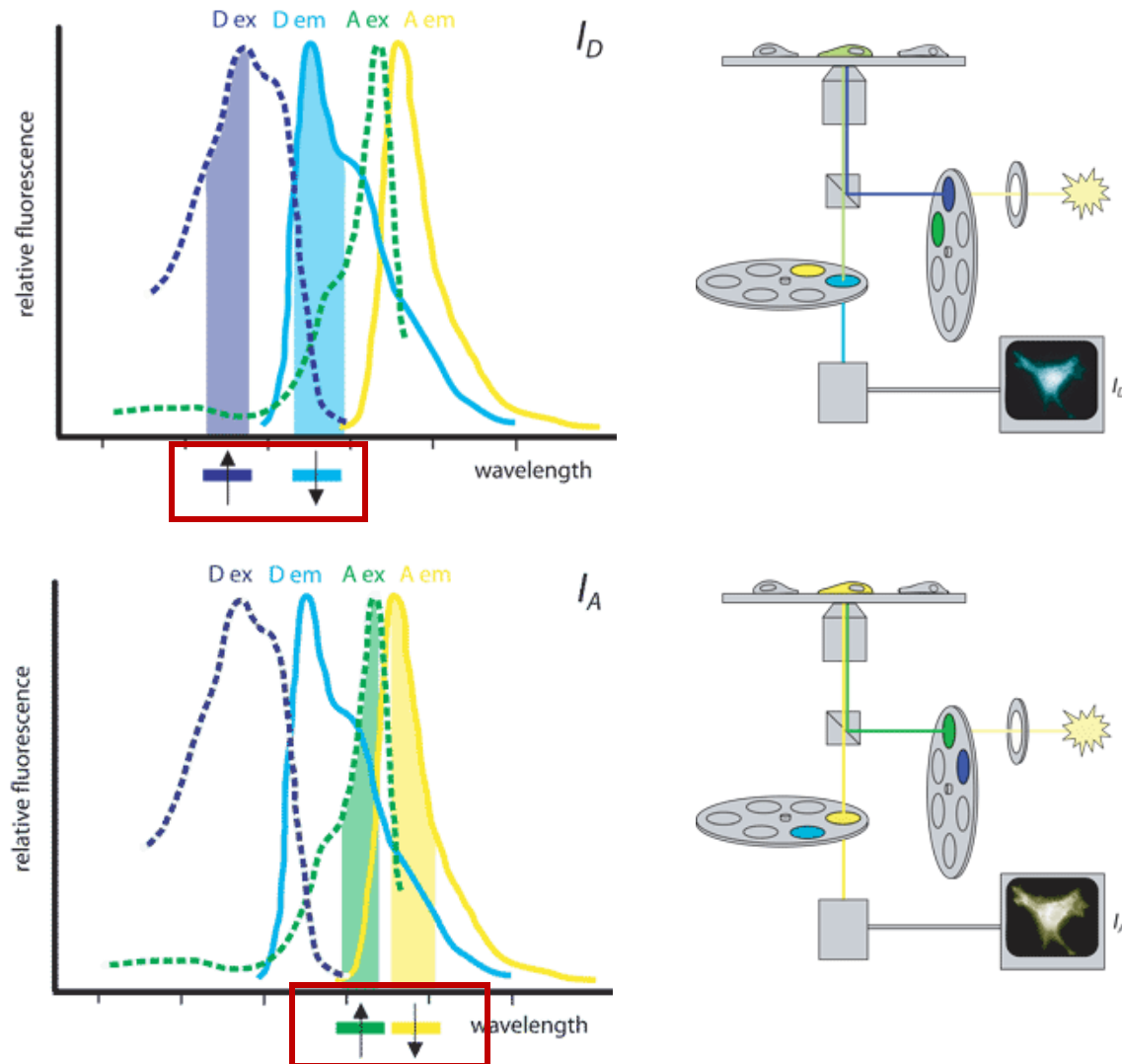
## 1. SENSITIZED EMISSION



Donor is excited by a specific wavelength and the signal is collected by using emission filters chosen for the donor and the acceptor fluorescence

# Methods for imaging FRET

## 1. SENSITIZED EMISSION

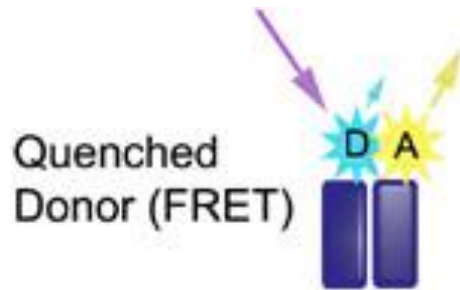


Appropriate controls to correct for the cross-talk between excitation and emission of the fluorophores

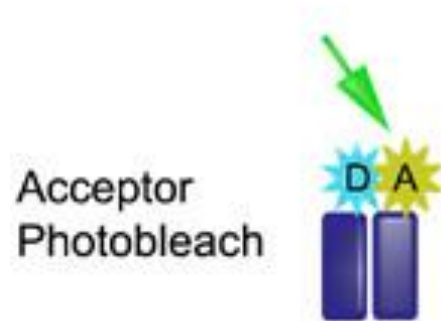


# Methods for imaging FRET

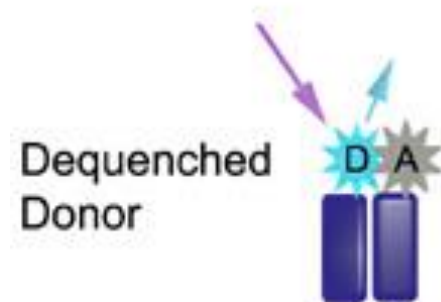
## 2. ACCEPTOR PHOTOBLEACHING



The donor fluorescence is quenched owing to FRET because some of the donor fluorescence energy is used to make acceptor fluorescence.



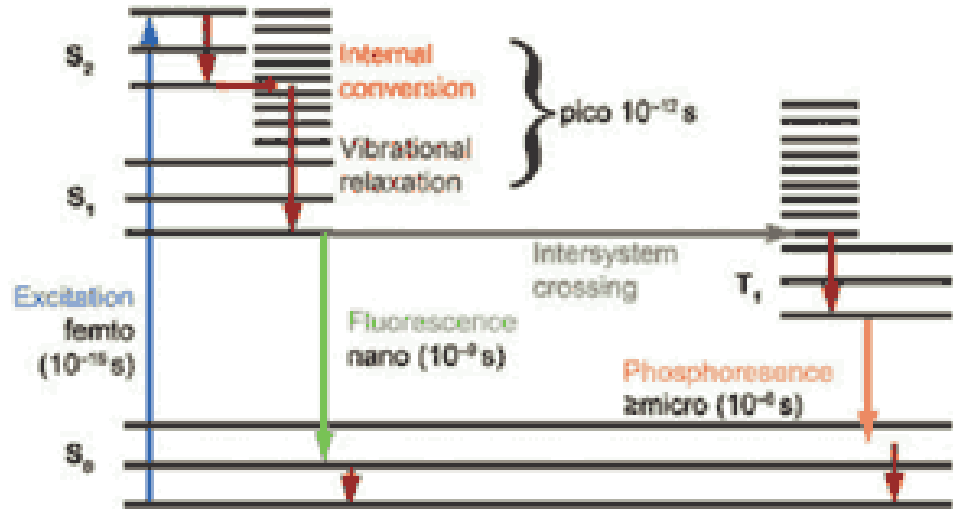
**Photobleaching the acceptor** fluorophore releases this quenching and **increases the donor fluorescence**



For these experiments it is important to ensure that the acceptor photobleaching does not degrade the donor

# Methods for imaging FRET

## 3. FLIM (Fluorescence Lifetime Imaging Microscopy)



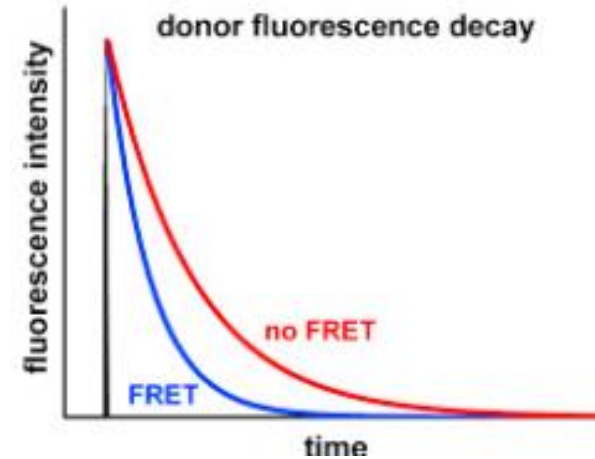
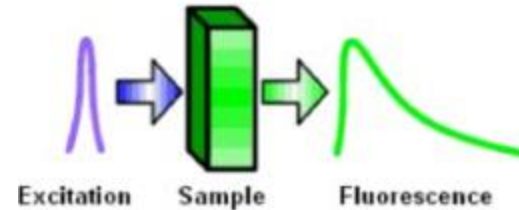
### Fluorescence lifetime:

time it takes an electron in an excited energy level of the dye molecule to return to its ground level while emitting fluorescence light

It depends on molecule environment: **if there are alternative routes to fluorescence to depopulate the excited energy state, the measured lifetime is reduced.**

# Methods for imaging FRET

## 3. FLIM (Fluorescence Lifetime Imaging Microscopy)



The donor fluorescence is quenched by FRET and the amount of quenching can be determined by measuring the shortening of fluorescence decay of the donor in the presence of FRET.

Advantages: less prone to cross-talk artifact because it looks only at the donor fluorescence. FLIM is not so sensitive to direct acceptor excitation artifacts.

Disadvantages: expensive instrumentation; low temporal resolution (potentially several min/image)

- Studies of molecular dynamics in live cells
- ✓ **FRAP**: Fluorescence Recovery After Photobleaching
- ✓ **FLAP**: Fluorescence Localization After Photobleaching
- ✓ **FLIP**: Fluorescence Loss of Intensity after Photobleaching

# Photobleaching

Photobleaching is the photochemical destruction of a fluorophore.

Photobleaching occurs when a fluorophore permanently loses its ability to fluoresce due to photon-induced chemical damage and covalent modification.

Photobleaching Rates in Multiply Stained Specimens

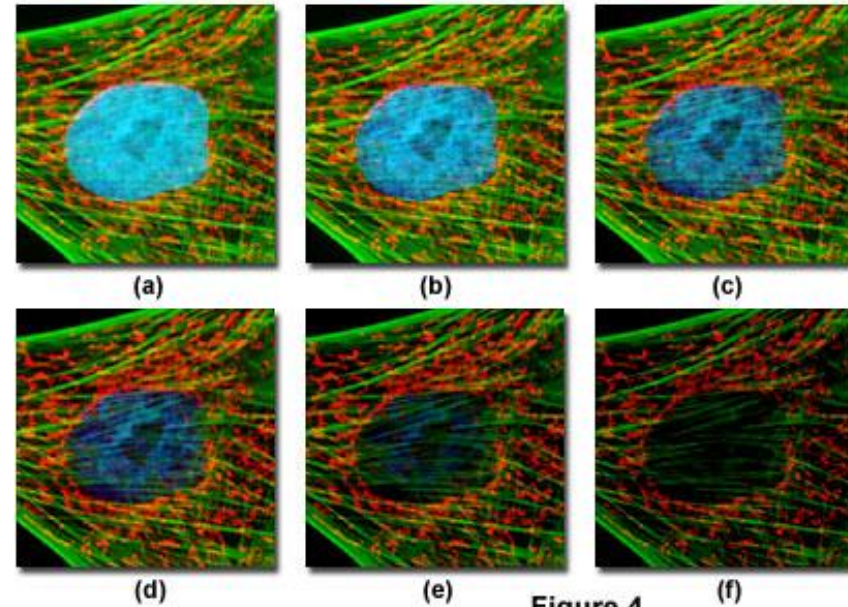
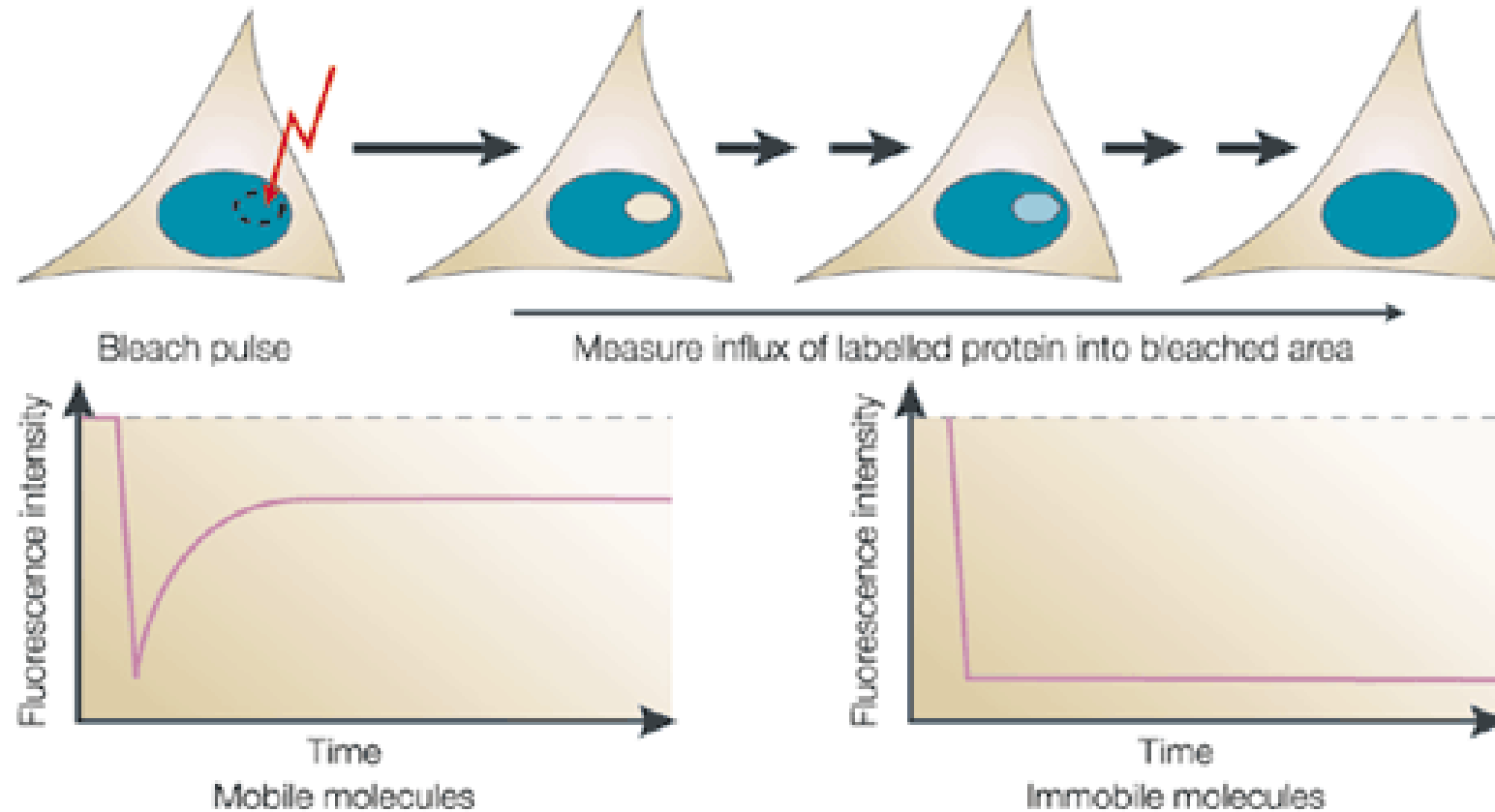


Figure 4

# FRAP

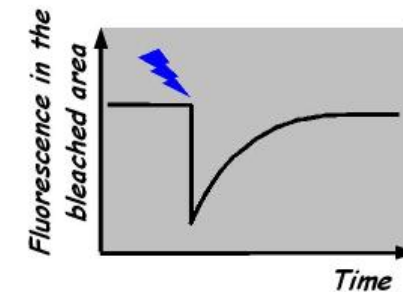
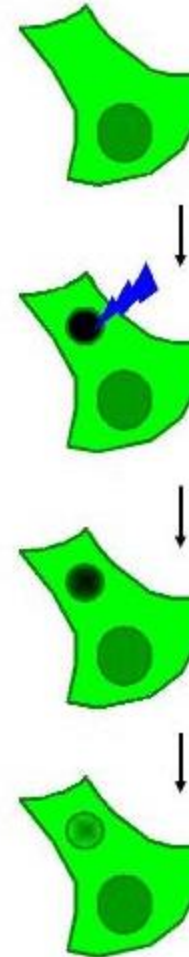
## Fluorescence Recovery After Photobleaching



FRAP is used to measure the dynamics of 2D or 3D molecular mobility e.g. diffusion, transport or any other kind of movement of fluorescently labeled molecules in living cells.

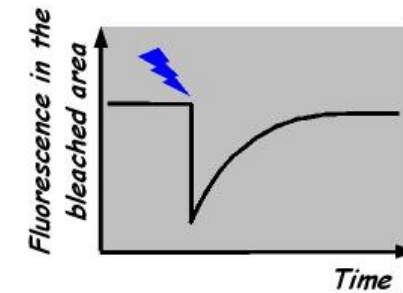
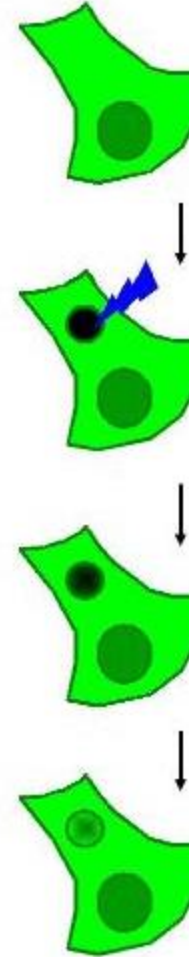
# Execution of FRAP experiment

1. Label the protein of interest with a fluorescent probe (e.g. GFP)
2. Choose a ROI and save some background images of the sample before photobleaching
3. Apply short high intensity local bleach: the fluorophores in this region receive high intensity illumination which causes their fluorescence lifetime to quickly elapse. Now the image in the microscope is that of a uniformly fluorescent field with a noticeable dark spot



# Execution of FRAP experiment

4. Take images after bleaching until the recovery in the bleach area reach a plateau. As Brownian motion proceeds, the still-fluorescing probes will diffuse throughout the sample and replace the non-fluorescent probes in the bleached region.





The mean intensity in the ROI is plotted versus time, where the level of fully recovered intensity gives information on mobile/immobile species of the fluorescent molecule.

Mobile Fraction: fraction of fluorescent protein that can diffuse into the bleached area during the time course of the experiment

$$F_m = I_E / I_I$$

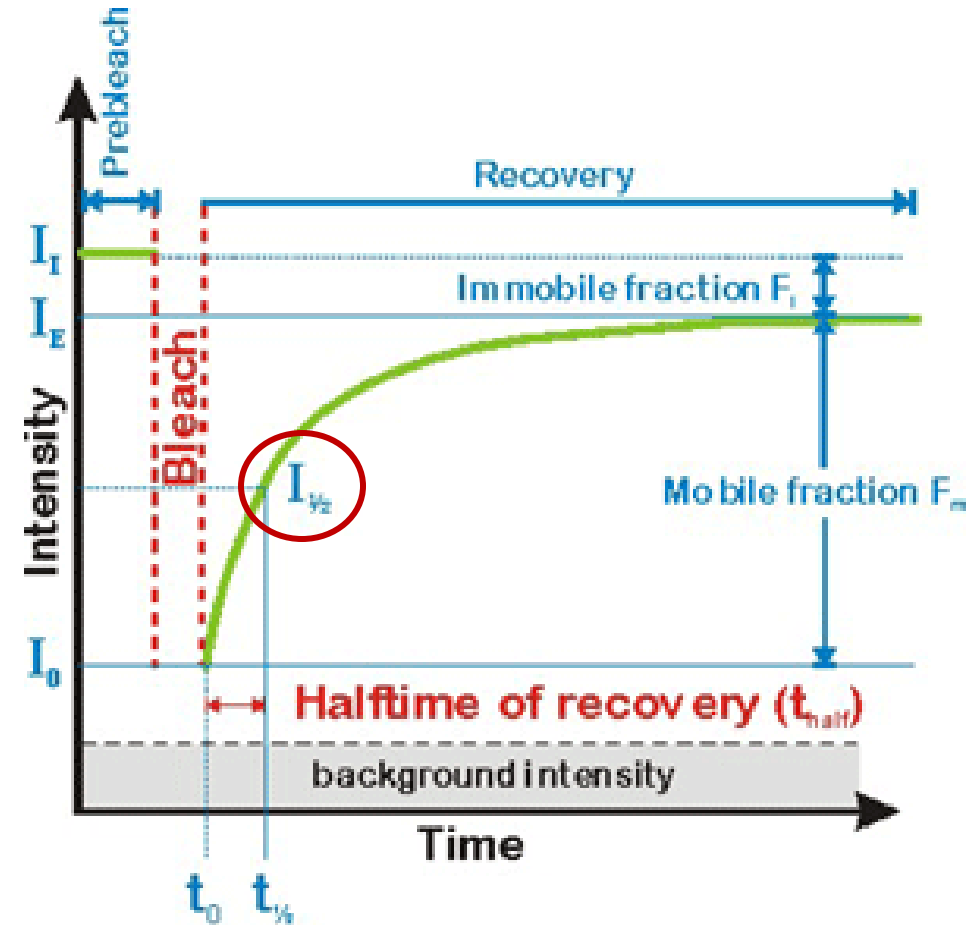
The recovery time (half-time) indicates the speed of this mobility, e.g. diffusion time;

This diffusion proceeds in an ordered fashion, analytically determinable from the diffusion equation. Assuming a gaussian profile for the bleaching beam, the diffusion constant D can be simply calculated from:

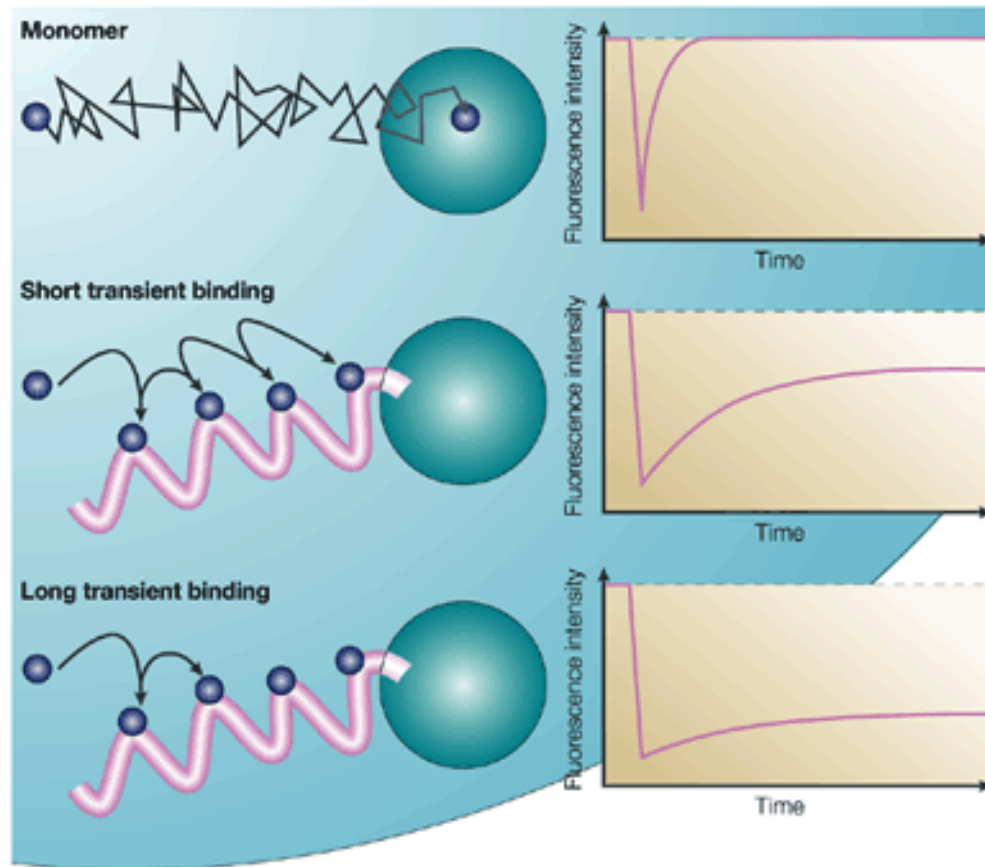
$$D = \frac{w^2}{4t_{1/2}}$$

w = width of the beam

$t_{1/2}$  = time required for the bleach spot to recover half of its initial intensity



The fluorescence intensity versus time plot can give us information about diffusion properties of the molecule of interest.



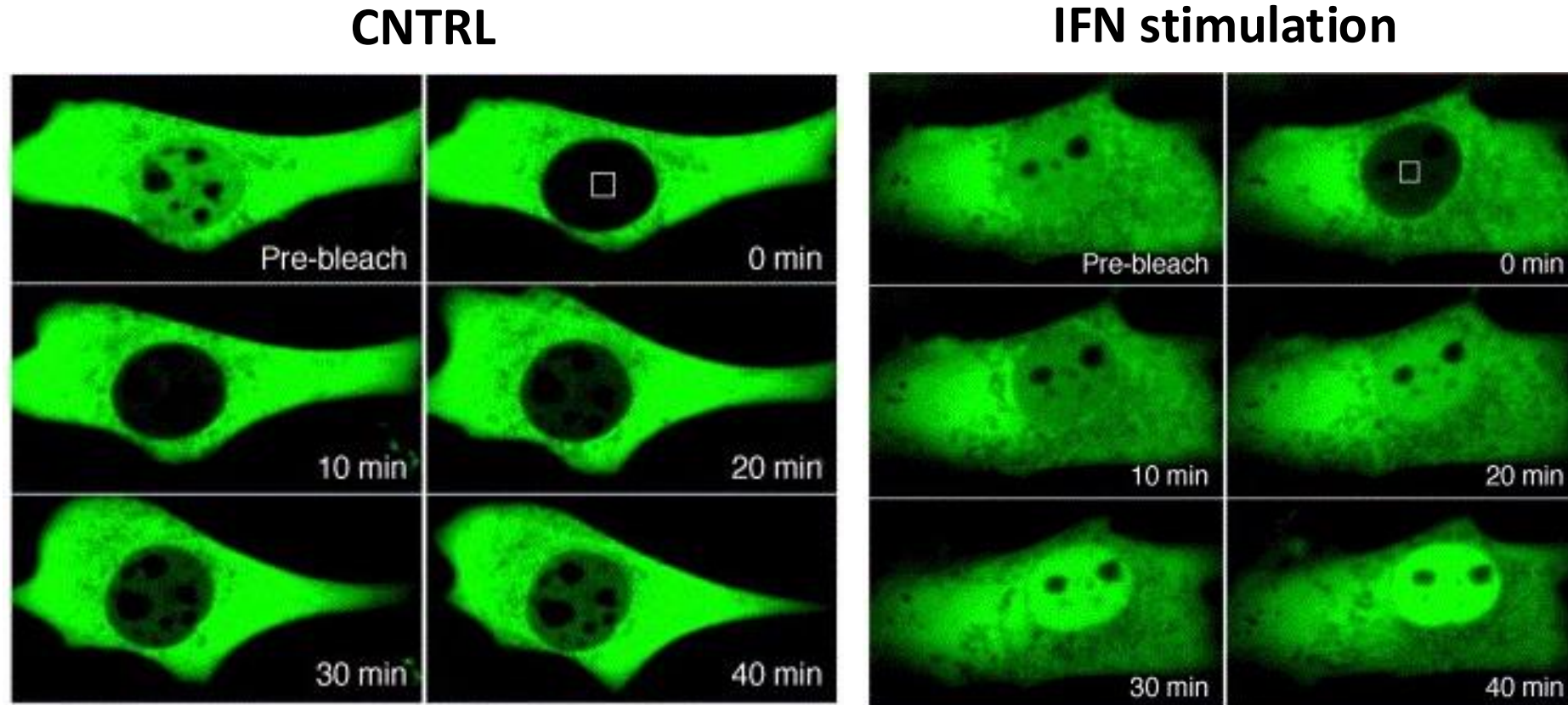
## protein binding versus free diffusion *in vivo*.

As all proteins readily interact with many partners *in vivo*, it is virtually impossible to measure pure diffusional mobility of a protein in a living cell.

The fact that the interaction properties of a protein are reflected in the mobility measurement complicates the analysis of photobleaching data.

Kinetic modelling allows us to extract information about the binding properties from mobility measurements.

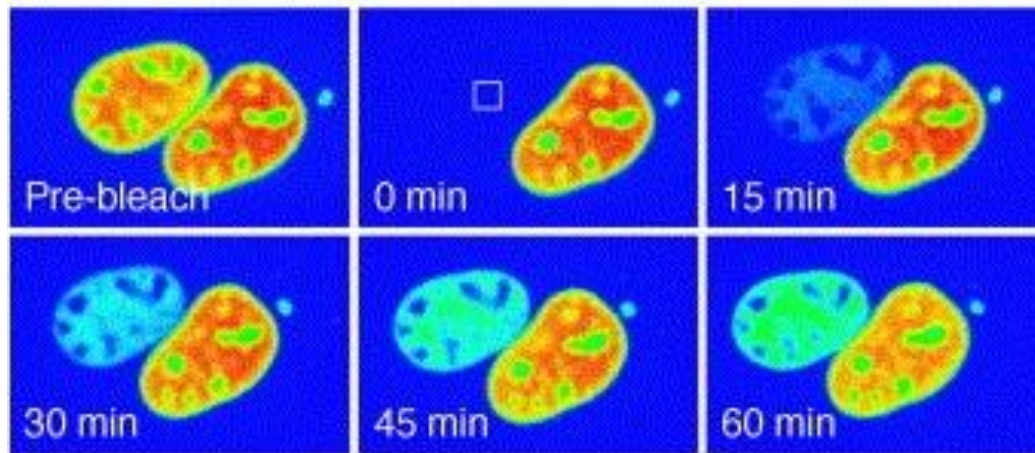
# Application of FRAP to nucleocytoplasmic shuttling



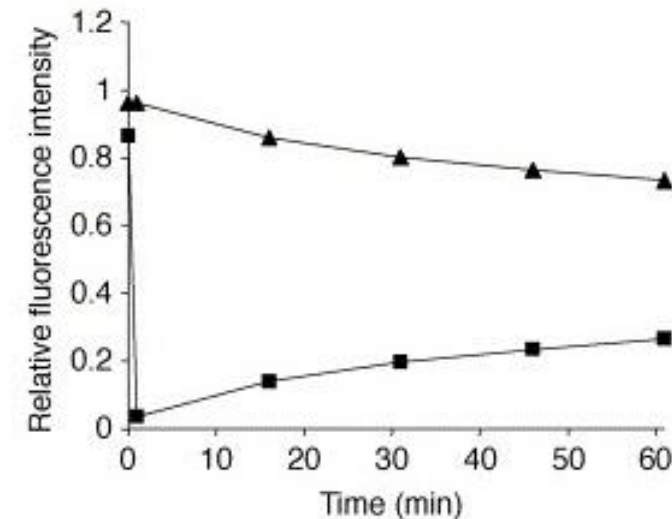
Koster M. *et al.*, *Curr Opin in Biotech*, 2005, 16: 28-34

Qualitative FRAP analysis to determine the kinetics of constitutive and stimulated nucleocytoplasmic transport of STAT1–EGFP in NIH3T3 cells

# Application of FRAP to nucleocytoplasmic shuttling



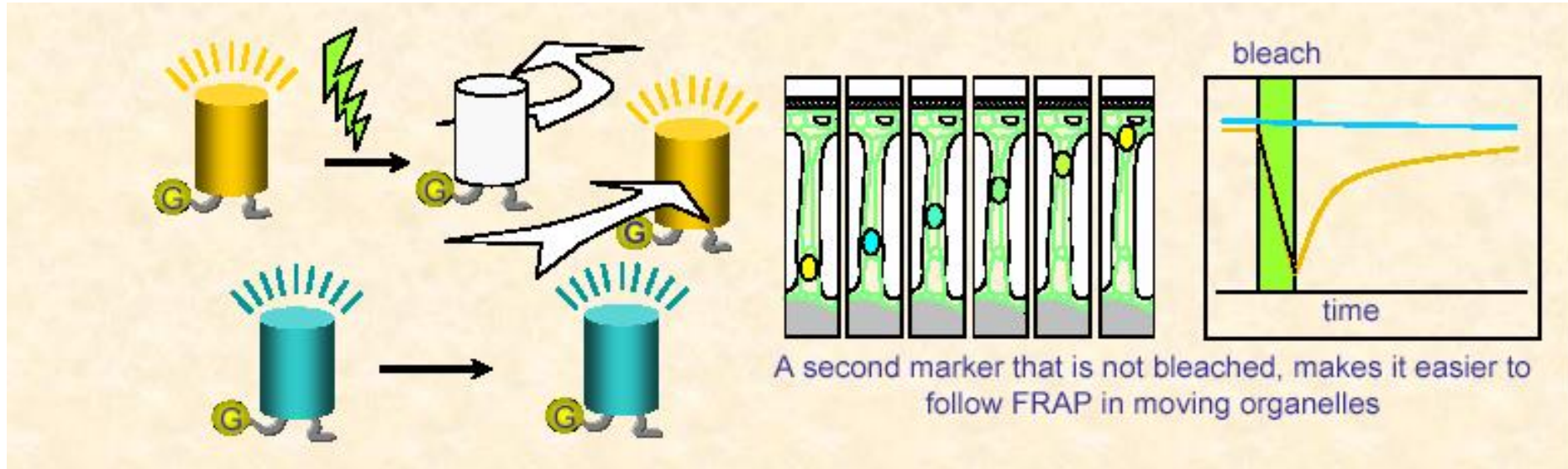
After bleaching of one nucleus the recovery of STAT1–EGFP during ongoing signaling was monitored for 60 min. Fluorescence intensities of the entire unbleached and bleached nucleus were measured and corrected for background intensity.



Koster M. *et al.*, *Curr Opin in Biotech*, 2005, 16: 28-34

# FLAP

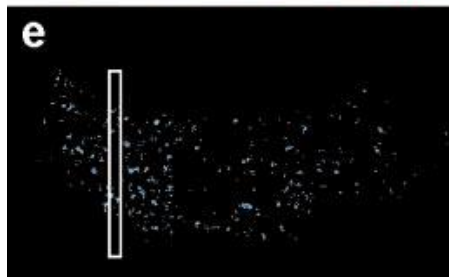
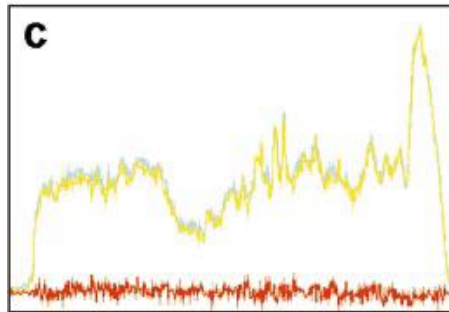
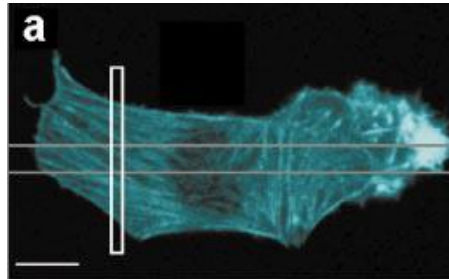
## Fluorescence Localization After Photobleaching



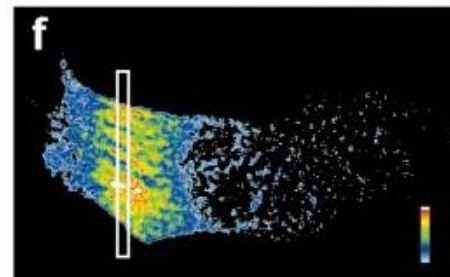
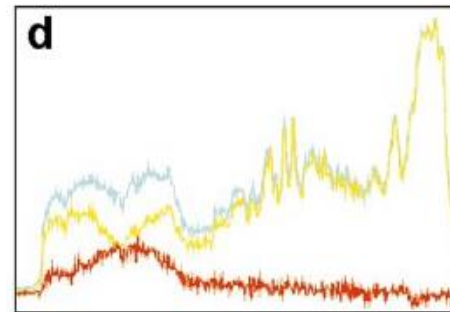
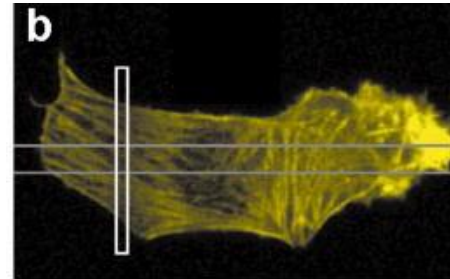
The molecular species to be located carries two different fluorophores that can be imaged independently but simultaneously by fluorescence microscopy. One of the fluorophores **YFP** (the **target fluorophore**) is then rapidly photobleached at a chosen location. The unbleached **CFP** (**reference**) fluorophore remains colocalized with the target fluorophore; thus, the subsequent fate of the photobleached molecules can be revealed by processing simultaneously acquired digital images of the two fluorophores.

# Application of FLAP to actin replacement dynamics

CFP-actin



YFP-actin



Confocal microscopy revealed that **the two fluorophores are accurately co-localized within the cells** and thus that the intensity difference (**the FLAP signal**) is close to zero throughout the image

**Photobleaching YFP** give rise to a **strong FLAP signal**.

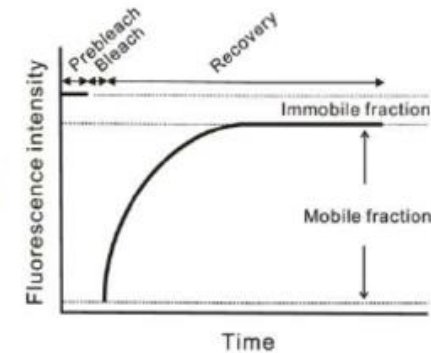
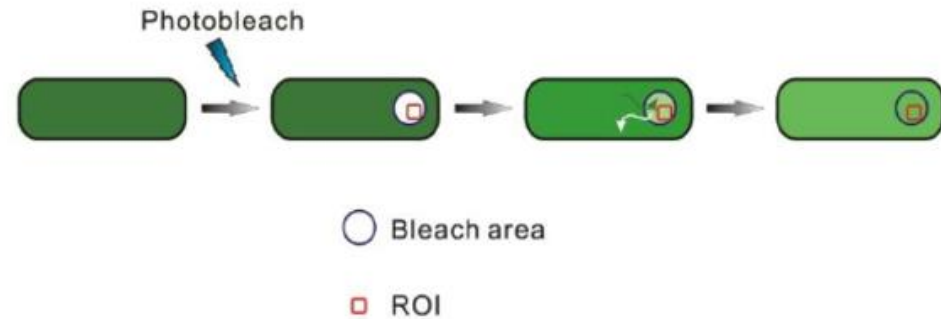
Immediately after bleaching a diffuse low-level signal had uniformly filled the local cytoplasm of the cell but not the cell nucleus

Dunn *et al.*, J Microscopy. 2002; 205:109-112.

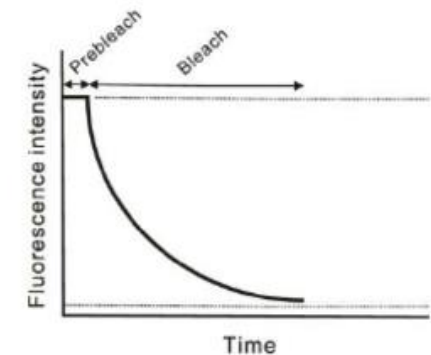
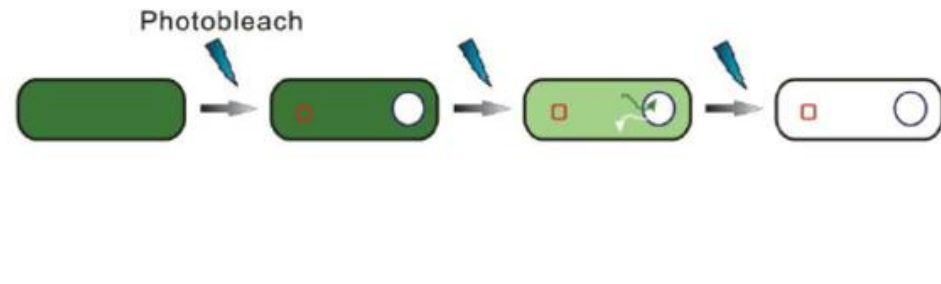
# FLIP

## Fluorescence Loss of Intensity after Photobleaching

### FRAP



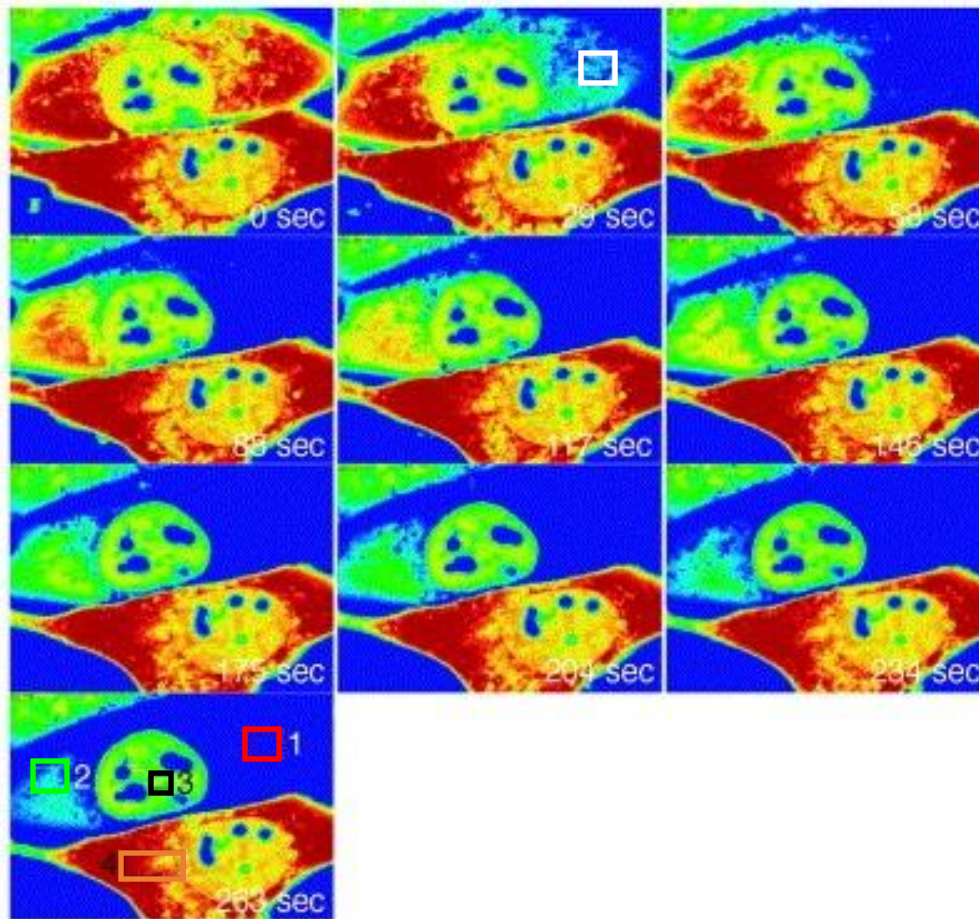
### FLIP



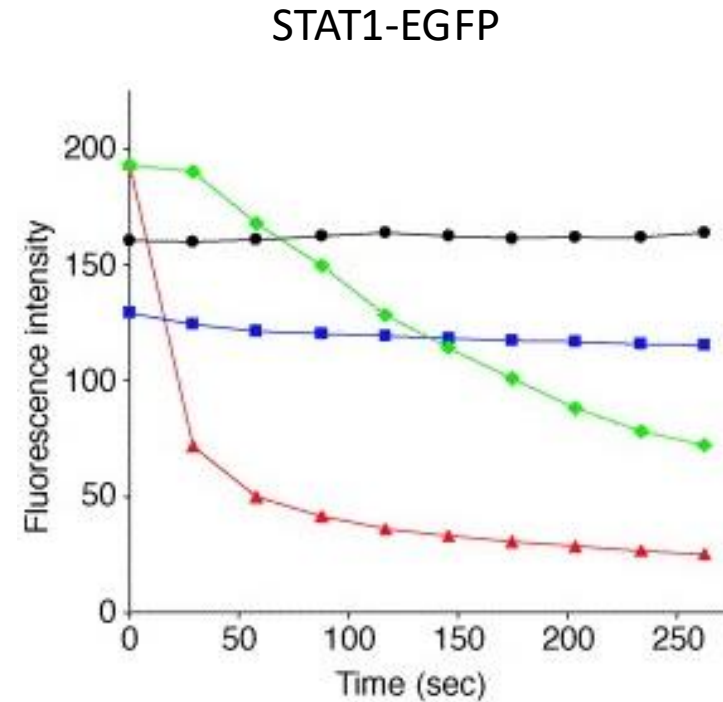
An area within the cell is repeatedly bleached and the loss of fluorescence in areas that are distant from the bleach area is monitored.





FLIP largely eliminates the concern that the recovery properties are due to damage at the bleach spot, as all measurements are made in areas that are never bleached.

# Application of FLIP to nucleocytoplasmic shuttling



Koster M. *et al.*, *Curr Opin in Biotech*, 2005, 16: 28-34



-  bleached cytoplasmic area
-  unbleached cytoplasmic area
-  nucleus
-  reference cell

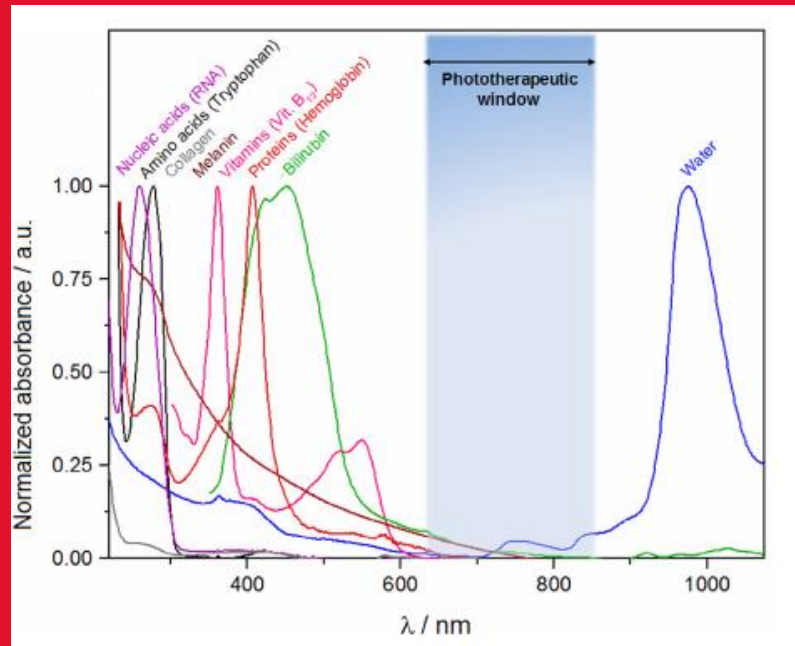


# BIOMEDICAL APPLICATIONS



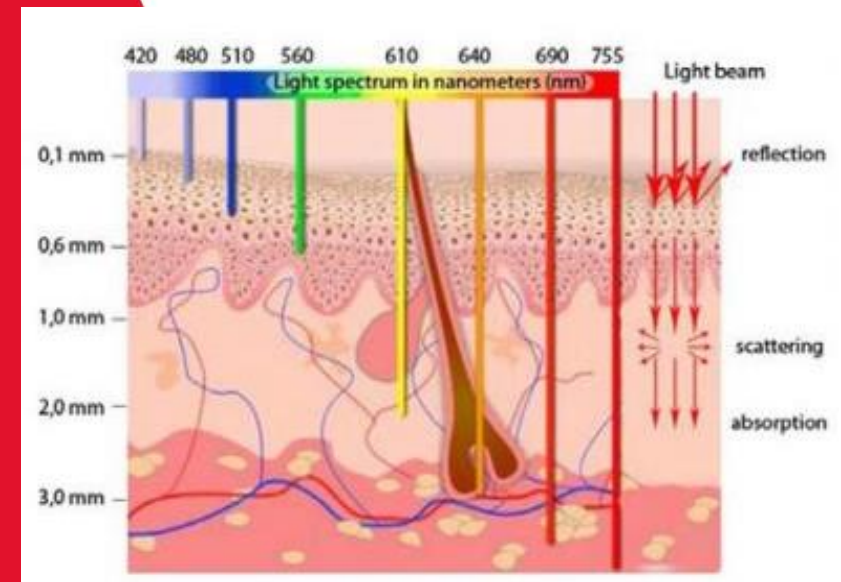
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and Systems Biology

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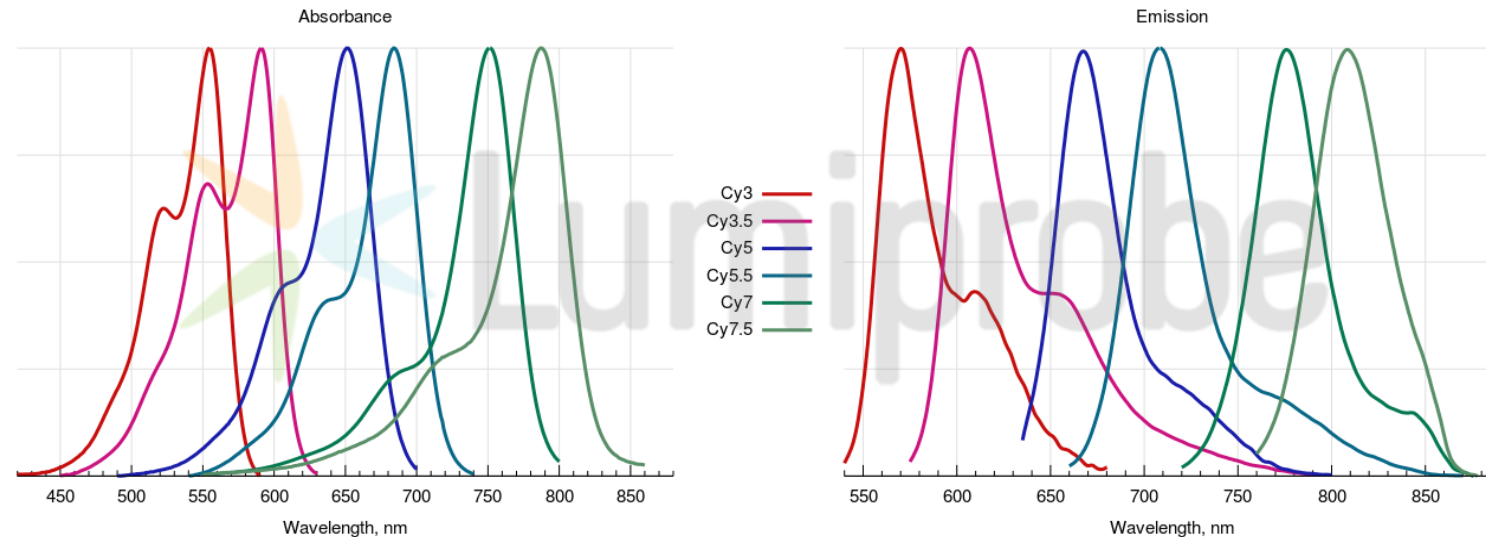
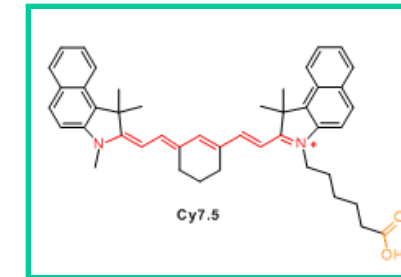
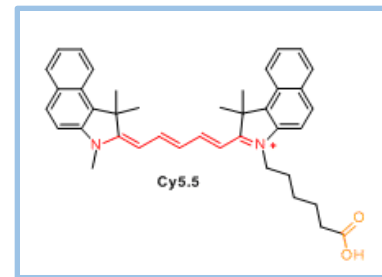
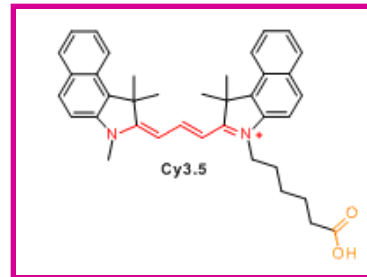
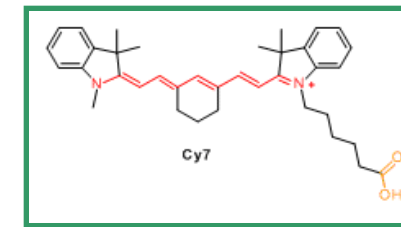
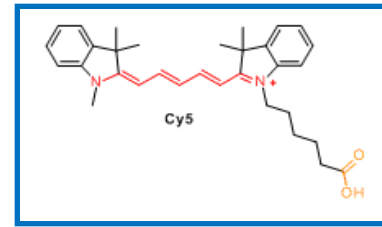
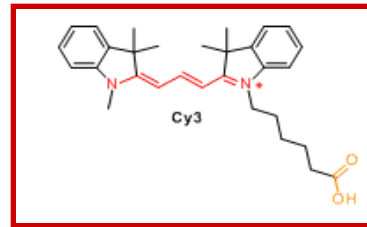


- high molar extinction coefficient ( $\epsilon$ )
- absorption in the red and near infrared region (650-850 nm)

- stability and solubility in physiological environment
- optimal ADME (Absorption, Distribution, Metabolism, Excretion)

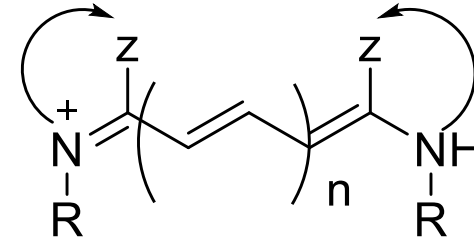


# POLYMETHINE DYES



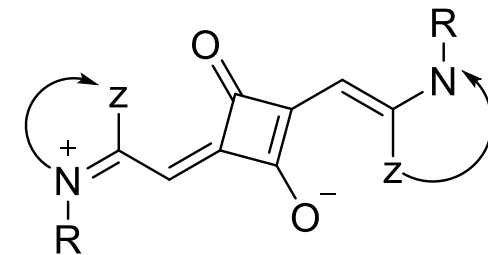
# POLYMETHINE DYES

- Excellent optical properties (high  $\epsilon$  and  $\phi$ )
- High structural versatility
- Tunable spectral properties
- Wide application fields



Cyanines

- Good biocompatibility at effective concentrations
- Good cellular uptake
- Preferential accumulation in tumor tissues



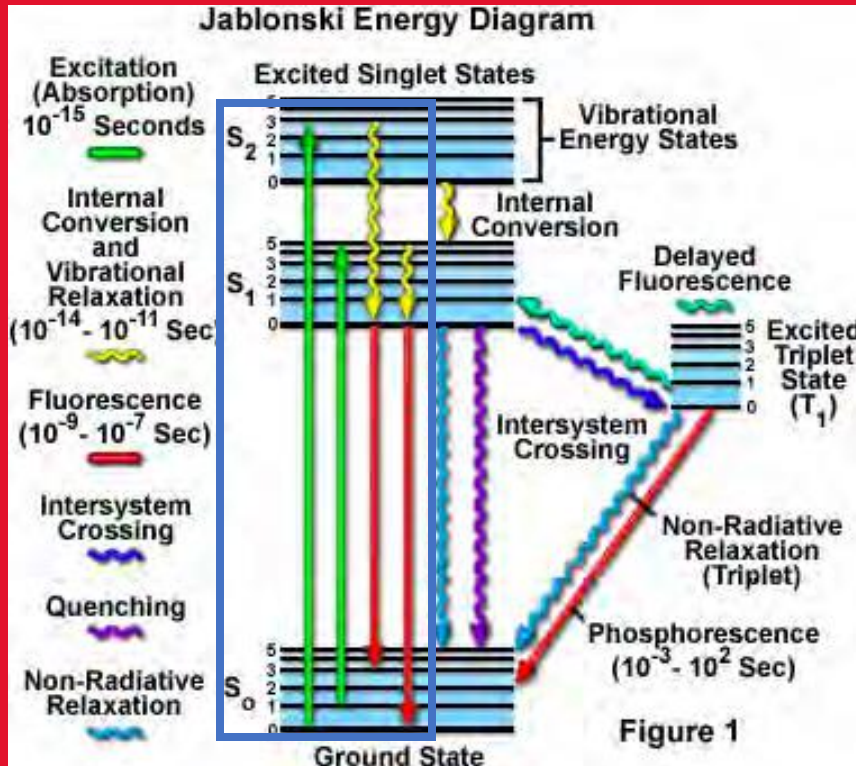
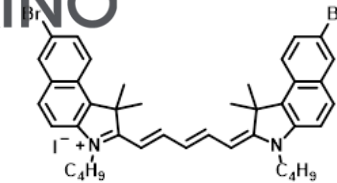
Squaraines

# DIAGNOSTIC TOOLS FOR *IN VIVO* IMAGING



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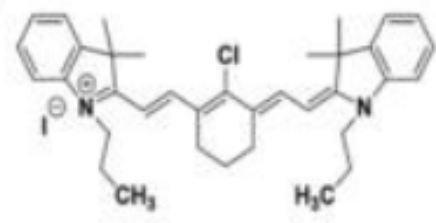


Normalized  
intensity

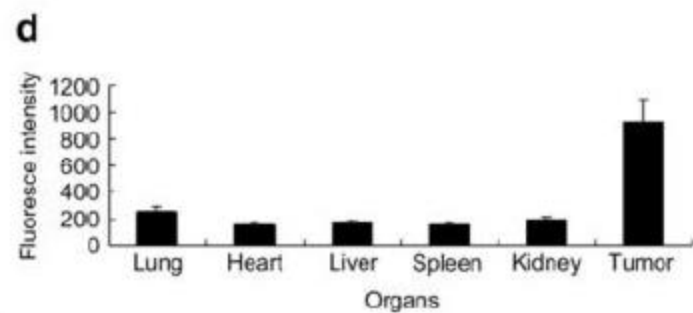
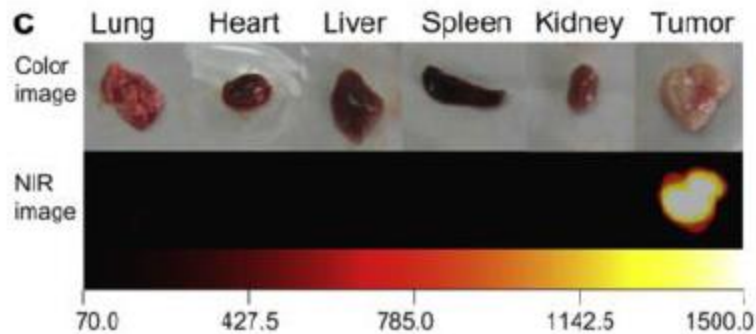
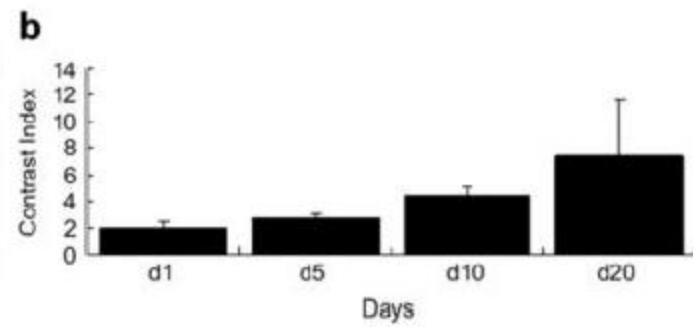
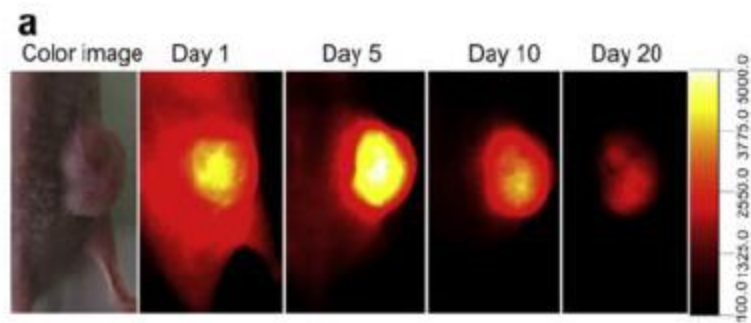
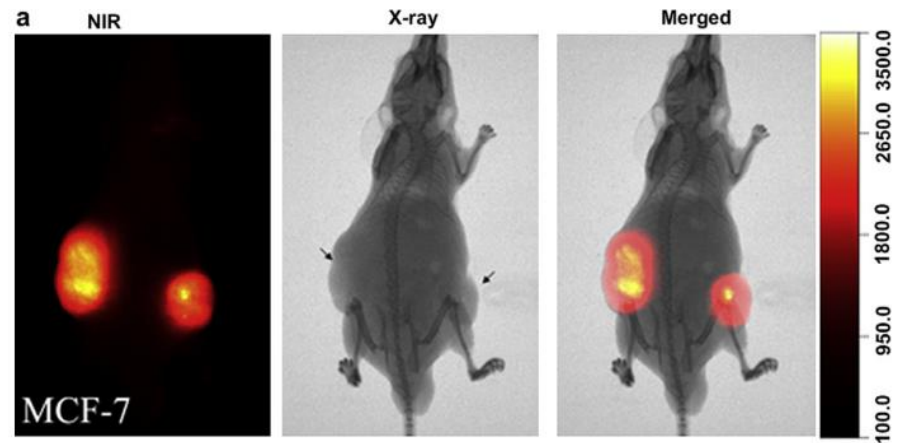


$$\epsilon_{\text{EtOH}} = 208\,538 \text{ M}^{-1}\text{cm}^{-1}$$

$$\Phi_{\text{DMSO}} = 36,6 \%$$



IR-780

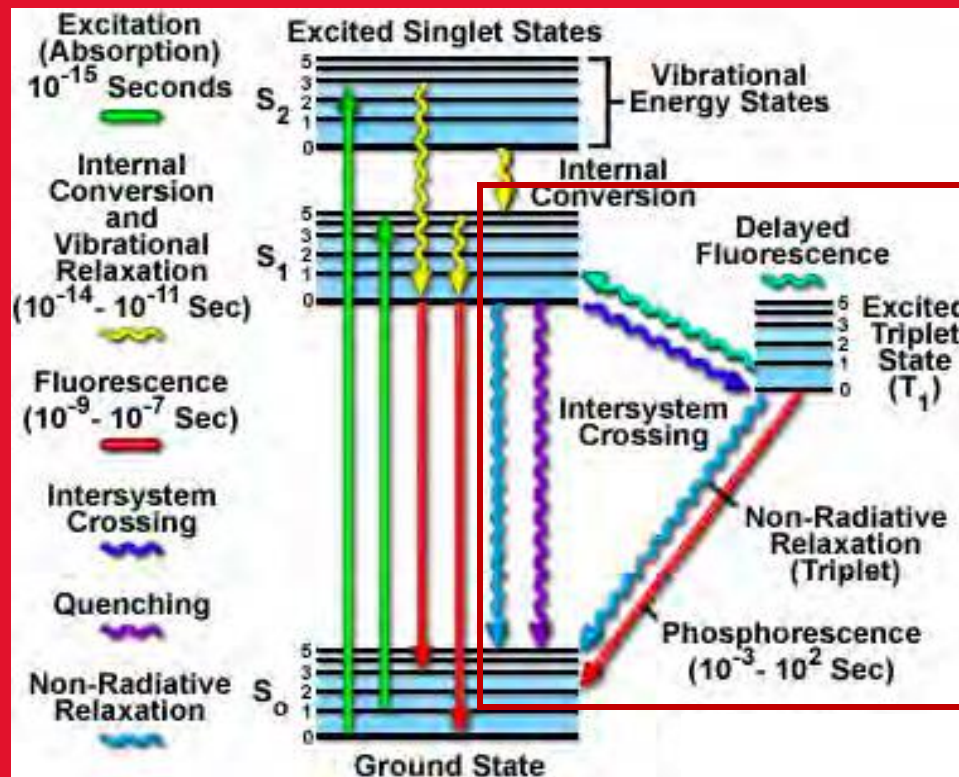


Tan et al., *Biomaterials* **33**, 2230-2239 (2012)



# PHOTODYNAMIC THERAPY

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Type I photochemistry:  
**Electron/hydrogen  
transfer**

**RADICAL  
OXIGEN  
SPECIES**

Type II photochemistry:  
**Energy transfer  
(to molecular oxygen)**

$^1O_2$

**Photochemical reaction**

# Photodynamic therapy (PDT)

is a minimally invasive and minimally toxic light-based treatment used in medicine to treat a wide range of clinical conditions

## Advantages

Technique FDA-approved

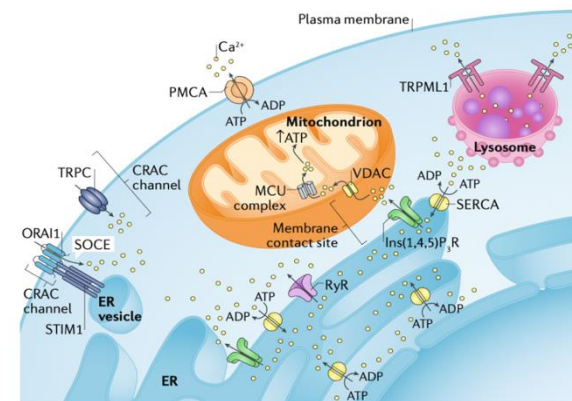
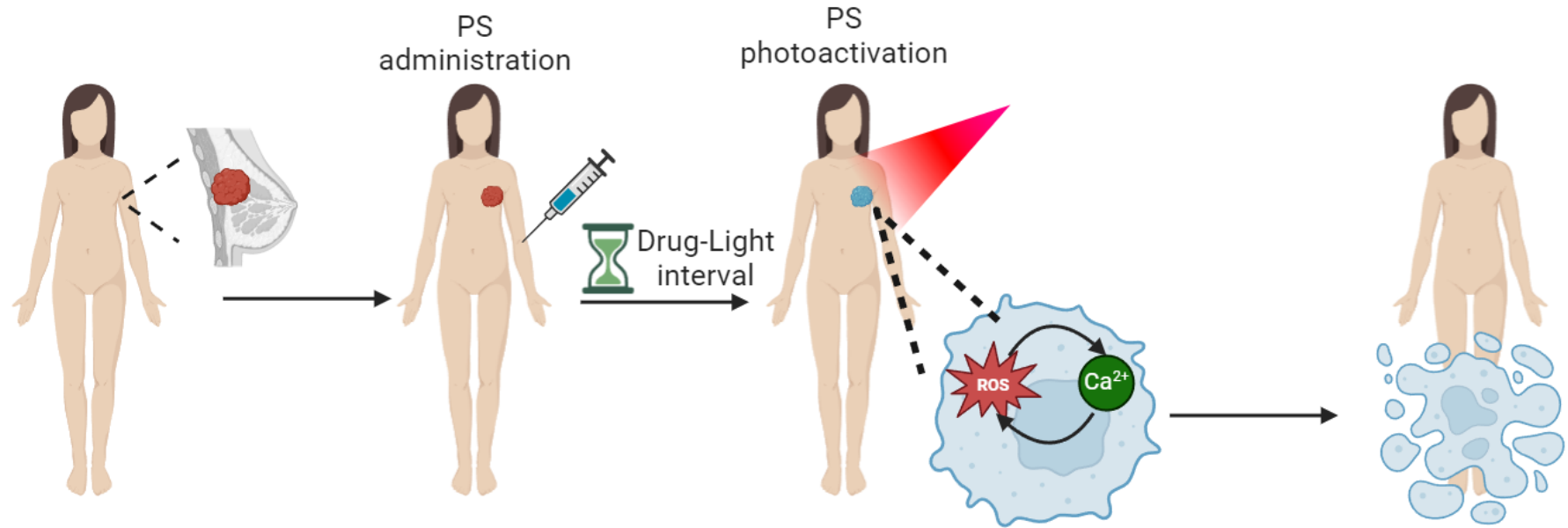
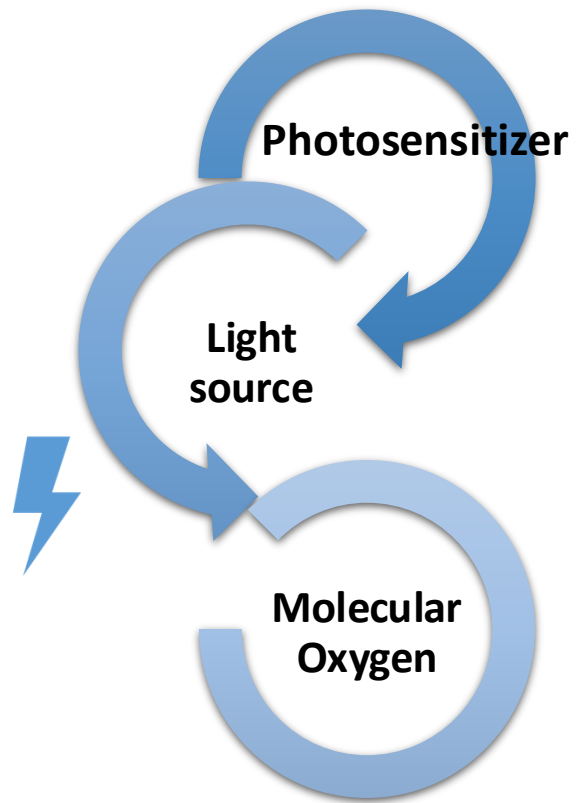
Localized therapy

Minimally invasive

Few collateral effects

Possibility to combine it with conventional anti-cancer therapies

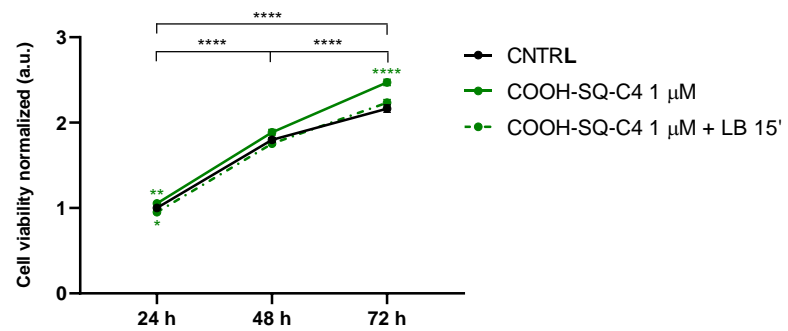
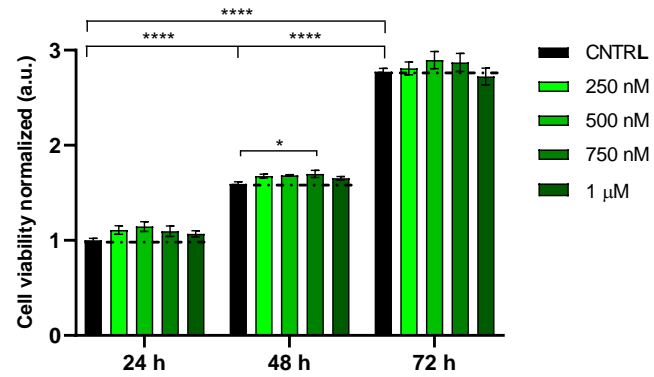
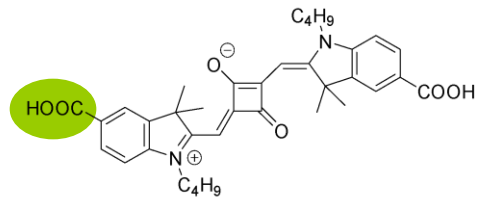
# How does PDT work?



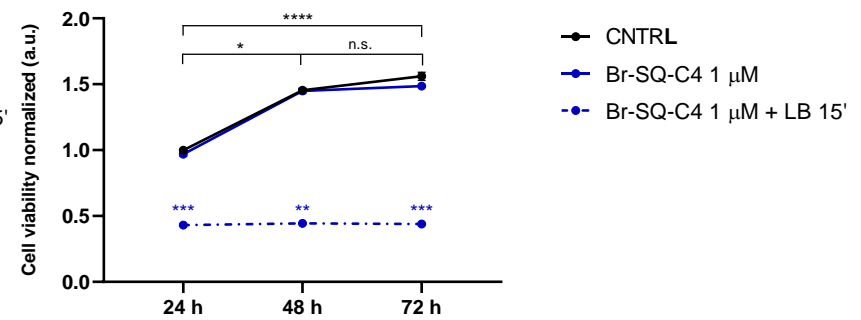
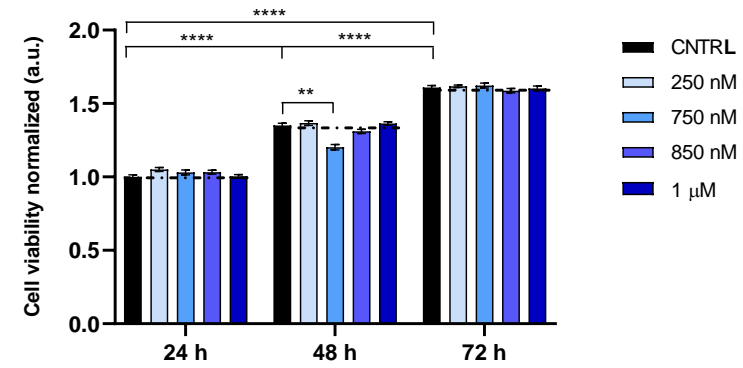
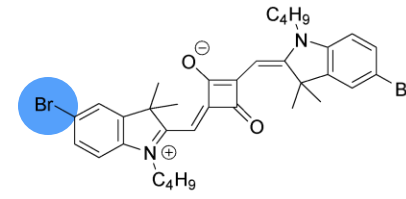
Giorgi C. et al.(2018)

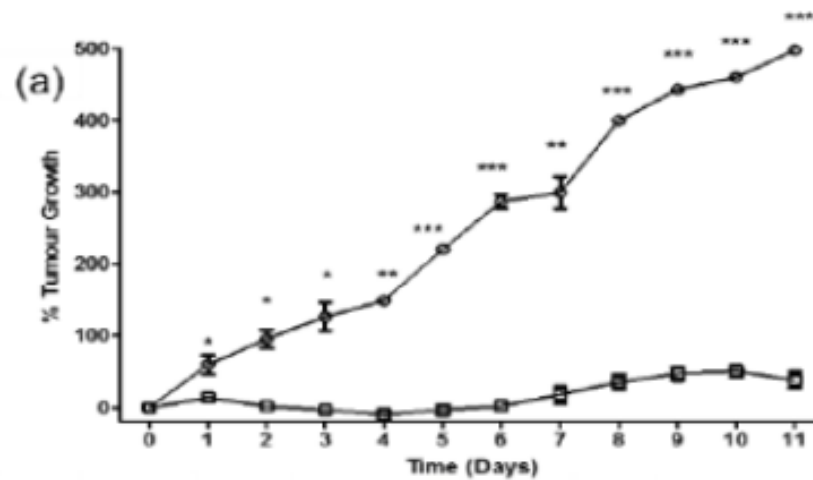
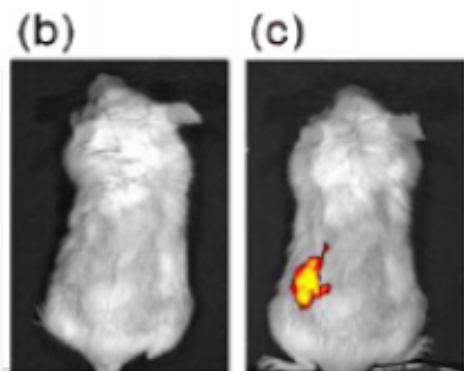
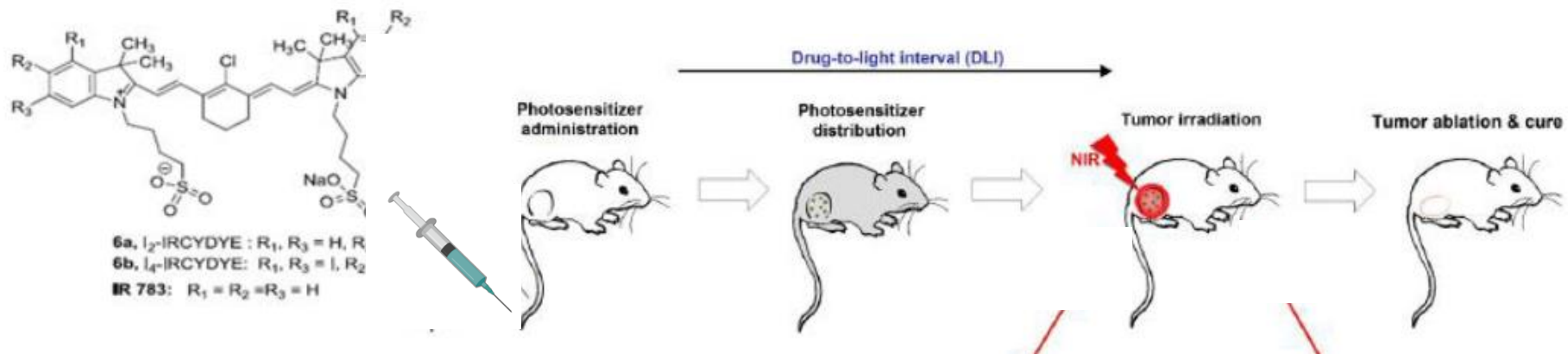


## COOH-SQ-C4



## Br-SQ-C4





Atchison *et al.*, *Chem. Commun.* **53**, 2009-12 (2017)



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**Thank you**